Multi-institutional Collaborations for Improving Deep Learning-based Magnetic Resonance Image Reconstruction Using Federated Learning ——Supplementary Material——

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1. Supplementary Introduction

In this supplementary document, we first provide supplementary method including details of network architecture and addition schematics of FL-MRCM. Then, we present additional experimental results including experiments on different acceleration factors, more qualitative results, and ablation studies.

2. Supplementary Method

We use a U-Net [4] style encoder-decoder architecture for the reconstruction networks. Table 1 shows the details of each block in encoder and decoder in our reconstruction network. Note Conv and ConvTranspose denote the 2D convolution and 2D transposed convolution operator, respectively. The encoder networks can be described as follows:

ConvBlock(1,32)-AvgPool(2,2)-ConvBlock(32,64)-AvgPool(2,2)-ConvBlock(64,128)-AvgPool(2,2)-ConvBlock(128,256)-AvgPool(2,2)-ConvBlock(256,512),

where AvgPool(2,2) represents 2D average pooling with kernel size of 2 and stride size of 2 and other network modules are express by (in-channel, out-channel). Then, feature maps are projected to latent space as the input of domain identifiers by an adaptive average pooling layer with outshape $512 \times 2 \times 2$. The decoder networks can be expressed as follows:

Upsample(512,256)-ConvBlock(512,256)-Upsample(256,128)-ConvBlock(256,128)-Upsample(128,64)-ConvBlock(128,64)-Upsample(64,32)-ConvBlock(64,32)-Conv(32,1).

The domain identifier consists of two fully connected layers as follow:

FC(2048,256)-LeakyRelu(0.2)-FC(256,2),

where LeakyRelu(0.2) represents the LeakyRelu activation with negative slope of 0.2.

Figure 1 shows a global view of proposed FL-MRCM for multi-institutional collaborations in MR image reconstruction task. For the target site, the decoder part (green block) and the ground truth image are transparent, since they might be not involved during the training. As discussed in Section 4 of the main manuscript, there is not fully-sampled data for training in Scenario 1.

3. Additional Experimental Results

The ablation study about the effectiveness of proposed cross-site modeling is demonstrated by a set of the comparisons between FL-MR and FL-MRCM under the setting of federated learning. Furthermore, we also conduct a detailed ablation study to analyze the effectiveness of proposed cross-site modeling without federated learning framework for T_1 -weighted images. In this case, we obtain a trained model from one of available sites and evaluate the its performance on another institution to observe the gain purely contributed by cross-site modeling in Table 2. We present the experiment results when the acceleration factor is set to 8 in Table 4. Similar with results of acceleration factor of 4 in main manuscript, our proposed FL-MR exhibits better generalization and clearly outperforms other privacy-preserving alternative strategies. FL-MRCM outperforms FL-MR in each dataset by addressing the domain shift issue.

Table 5 is a extended version of Table 2 in the main manuscript. We additionally compare the performance of

Table 1. Configuration of Blocks in FL-MRCM

| Block | Layer | Kernel size | Stride | Padding | |
|-----------|---------------|-------------|--------|---------|--|
| | Conv | 3 | 1 | 1 | |
| | InstanceNorm | - | - | - | |
| ConvBlock | LeakyReLu | - | - | - | |
| CONVENER | Conv | 3 | 1 | 1 | |
| | InstanceNorm | - | - | - | |
| | LeakyReLu | - | - | - | |
| UpSample | ConvTranspose | 2 | 2 | 0 | |
| | InstanceNorm | - | - | - | |
| | LeakyReLu | - | - | - | |



Figure 1. The overview of the proposed FL-MRCM framework. Through several rounds of communication between data centers and server, the collaboratively trained global model parameterized by Θ_G^q can be obtained in a data privacy-preserving manner.



Figure 2. Bland-Altman plot corresponding to the fastMRI dataset between FL-MRCM and other methods in Scenario 1.

the proposed framework with models pre-trained with data from a single data center and then fine-tuned with data from target data center. In this case, we obtain a trained model from one of the institutions, then we transfer the pre-trained weights to the target site and fine-tune the pretrained model by the training data of the target site, which will not compromises the data sharing regulations. We denote this set of experiments as **Transfer** in Table 5. The reported results suggest that pre-trained on a large dataset (e.g., the F dataset) can improve the performance but the multi-institutional collaboration is still a better option if multiple datasets are available.

Figure 3 shows the qualitative performance of different methods on T_1 and T_2 -weighted images from four datasets

in Scenario 2. It can be observed that the proposed FL-MRCM method yields reconstructed images with remarkable visual similarity to the reference images compared to the other alternatives (see the last column of each sub-figure in Fig. 3) in four datasets with diverse characteristics.

To investigate the performance improvement of the proposed FL-MRCM, we conduct t-test based on the SSIM of the reconstructed images between FL-MRCM and other methods. Averaged p values of each group of experiments in two scenarios are presented in Table 3. A p value less than 0.05 is usually considered as statistically significant. The reported performance of FL-MRCM satisfies this criterion. To further demonstrate the performance of the proposed FL-MRCM, we show an example of Bland–Altman

| sing, the target site is the institution that provides testing data. | | | | | | | | | | |
|--|------|--------|----------|-----------|-------|------------------------|--------|---------|-------|--|
| Data Centers w/o | | | Cross-si | ite Model | ing | w/ Cross-site Modeling | | | | |
| (Institutions) | | SSIM | DENID | Average | | SSIM | DSND | Average | | |
| Train | Test | 55111 | 1 SINK | SSIM | PSNR | 55111 | 1 SINK | SSIM | PSNR | |
| В | F | 0.7694 | 28.61 | | | 0.7987 | 29.53 | | | |
| В | Н | 0.5188 | 25.07 | 0.7222 | 27.93 | 0.5350 | 25.08 | 0.7399 | 28.42 | |
| В | Ι | 0.8785 | 30.10 | | | 0.8859 | 30.65 | | | |
| F | В | 0.9016 | 34.65 | | | 0.9158 | 35.13 | | | |
| F | Н | 0.8402 | 28.52 | 0.8840 | 31.44 | 0.8603 | 28.83 | 0.8978 | 31.79 | |
| F | Ι | 0.9102 | 31.16 | | | 0.9172 | 31.42 | | | |
| Н | В | 0.6670 | 29.12 | | | 0.7256 | 31.54 | | | |
| Н | F | 0.8571 | 31.82 | 0.7736 | 30.03 | 0.8938 | 32.59 | 0.8292 | 31.40 | |
| Н | Ι | 0.7968 | 29.16 | | | 0.8681 | 30.07 | | | |
| Ι | В | 0.8795 | 33.76 | | | 0.9310 | 35.03 | | | |
| Ι | F | 0.8417 | 31.18 | 0.7831 | 30.68 | 0.8803 | 31.81 | 0.8522 | 31.58 | |
| I | Н | 0.6281 | 27.09 | | | 0.7454 | 27.89 | | | |

Table 2. Quantitative ablation study of proposed cross-site modeling on T_1 -weighted images. For experiments with cross-site modeling, the target site is the institution that provides testing data.

plot for fastMRI (the largest dataset) in Fig. 2. The y axis represents the SSIM difference of the reconstructed images between FL-MRCM and other methods. We can observe that most points lie in the positive range, which implies that FL-MRCM exhibits better reconstruction performance on most subjects.

Table 3. The p values of t-test among different methods in two scenarios.

| | Scenario 1 | | | Scenario 2 | |
|---------|------------------------|------------------------|---------|------------------------|------------------------|
| Method | T_1 -weighted | T_2 -weighted | Method | T_1 -weighted | T_2 -weighted |
| Cross | 4.11×10^{-27} | 2.76×10^{-07} | Single | 3.20×10^{-02} | 7.92×10^{-03} |
| Fused | 9.51×10^{-20} | 1.12×10^{-15} | FL-MR | 2.20×10^{-02} | 4.34×10^{-07} |
| FL-MR | 5.28×10^{-05} | 6.47×10^{-03} | FL-MRCM | - | - |
| FL-MRCM | - | - | - | - | - |

While our proposed method yields better performance, there are several limitations in our current study. First, experiments are conducted on the same sequences (e.g., T_1 and T_2) with the Cartesian undersampling. Although T_1 and T_2 are widely used sequences in clinical practice and Cartesian undersampling is usually adapted by compressed sensing, this might limit the applicability of our approach. The proposed method is inherently compatible with different kinds of sequences and undersampling. We will explore this direction in our future work. Second, experiments are based on simulated acquisition (starting from fully-sampled k-space and simulating acceleration). Further verification of accelerated acquisition on actual scanners will make this study more persuasive.

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Figure 3. Qualitative results of different methods that correspond to Scenario 2. For results of T_1 -weighted images on, (a) fastMRI [2], (b) HPKS, (c) IXI [1], (d) BraTS [3]. For results of T_2 -weighted images on, (e) fastMRI [2], (f) HPKS, (g) IXI [1], (h) BraTS [3]. The second row of each sub-figure shows the absolute image difference between reconstructed images and the ground truth.

Table 4. Supplementary quantitative comparisons with model trained by different strategies in Scenario 1. Here, acceleration factor is set to 8.

| Methods | Data Ce (Institut | nters ions) | | T_1 -we | eighted | | T_2 -weighted | | | |
|---------------|----------------------|----------------|--------|-----------|--------------|--------------|-----------------|-------|--------------|--------------|
| Wethous | Train | Test | SSIM | PSNR | Ave: SSIM | rage PSNR | SSIM | PSNR | Aver SSIM | rage PSNR |
| | F | В | 0.8920 | 30.62 | | | 0.8716 | 29.05 | | |
| | Н | В | 0.7242 | 27.88 | | | 0.7319 | 27.18 | | |
| | I | В | 0.8845 | 29.75 | | | 0.8089 | 27.30 | | |
| | | _ | | | | | | | | |
| | В | F | 0.6897 | 23.97 | | | 0.7162 | 23.76 | | |
| | Н | F | 0.8258 | 28.17 | | | 0.7948 | 25.42 | | |
| ~ | I | F | 0.7767 | 26.38 | | | 0.8057 | 26.37 | | |
| Cross | _ | | | | 0.7583 | 25.72 | | | 0.7583 | 25.72 |
| | В | Н | 0.3890 | 21.00 | | | 0.5280 | 22.84 | | |
| | F | Н | 0.7633 | 24.70 | | | 0.7966 | 26.33 | | |
| | I | Н | 0.5091 | 22.64 | | | 0.7837 | 26.01 | | |
| | | L. | 0.0100 | | | | 0.000 | 00.75 | | |
| | В | I | 0.8122 | 26.23 | | | 0.6802 | 23.75 | | |
| | F | I | 0.8548 | 27.60 | | | 0.8155 | 25.64 | | |
| | Н | 1 | 0.8029 | 26.66 | | | 0.7668 | 25.01 | | |
| | F, H, I | В | 0.8631 | 30.71 | 0.7701 | 27.41 | 0.8323 | 28.88 | 0.7966 | 26.76 |
| Fused | B, H, I | F | 0.8000 | 27.51 | | | 0.8214 | 26.25 | | |
| | B, F, I | н | 0.5607 | 23.74 | | | 0.7486 | 26.35 | | |
| | B, F, H | I | 0.8564 | 27.68 | | | 0.7840 | 25.58 | | |
| | F, H, I | B | 0.9005 | 31.22 | | | 0.8794 | 29.47 | 0.8380 | |
| FL-MR | B, H, I | F | 0.8598 | 29.14 | 0.8339 | 28.08 | 0.8517 | 26.95 | | 27.48 |
| | B, F, I | H | 0.7178 | 24.15 | | | 0.7965 | 27.13 | | |
| | B, F, H | 1 | 0.8574 | 27.80 | | | 0.8243 | 26.37 | | |
| | F, H, I | В | 0.9131 | 31.65 | | | 0.8868 | 29.51 | | |
| FL-MRCM | B, H, I | F | 0.8697 | 28.75 | 0.8473 | 28.28 | 0.8579 | 27.15 | 0.8479 | 27.57 |
| 12 111011 | B, F, I | н | 0.7440 | 24.72 | | -01-0 | 0.8145 | 27.18 | | |
| | B, F, H | 1 | 0.8625 | 28.01 | | | 0.8325 | 26.43 | | |
| | F, H, I | В | 0.9181 | 31.70 | | | 0.8866 | 29.30 | 0.8513 | |
| Mix | B, H, I | F | 0.8690 | 29.33 | 0.9545 | 28 15 | 0.8578 | 26.84 | | 27.45 |
| (Upper Bound) | B, F, I | H | 0.7726 | 24.94 | 0.0545 | 20.45 | 0.8265 | 27.25 | | |
| | B, F, H | I | 0.8581 | 27.85 | | | 0.8345 | 26.39 | | |

Table 5. Supplementary quantitative comparisons with models trained by different strategies in Scenario 2.

| Madaada | Data Cen (Institutio | iters ons) | | T_1 -we | eighted | | T_2 -weighted | | | |
|----------|------------------------------------|---------------|--------|-----------|---------|-------|-----------------|-------|----------|-------|
| Methous | Tain | Test | SSIM | PSRN | Average | | CCIM | DENID | Average | |
| | | iest | | | SSIM | PSNR | 33110 | PSNK | SSIM | PSNR |
| | В | В | 0.9660 | 37.30 | | 33.81 | 0.9558 | 34.90 | 0.9278 | 32.35 |
| Single | F | F | 0.9494 | 35.45 | 0.0351 | | 0.9404 | 32.43 | | |
| Single | Н | Η | 0.8855 | 29.67 | 0.9551 | | 0.9001 | 31.29 | | |
| | I | Ι | 0.9396 | 32.80 | | | 0.9151 | 30.79 | | |
| | B, F | F | 0.9453 | 34.97 | | | 0.9353 | 32.03 | | |
| | B, H | Н | 0.8861 | 29.76 | | | 0.9007 | 31.16 | | |
| | B, I | Ι | 0.9404 | 32.79 | | | 0.9119 | 30.65 | | |
| | F, B | В | 0.9669 | 37.33 | | | 0.9635 | 35.35 | | |
| | F, H | Н | 0.8948 | 30.05 | | | 0.9153 | 32.10 | - 0.9310 | 32.41 |
| Transfer | F, I | Ι | 0.9408 | 32.85 | 0.9355 | 33 72 | 0.9226 | 31.26 | | |
| mansier | H, B | В | 0.9638 | 36.59 | | 33.72 | 0.9566 | 34.47 | | |
| | H, F | F | 0.9445 | 34.99 | | | 0.9355 | 31.94 | | |
| | H, I | Ι | 0.9385 | 32.60 | | | 0.9162 | 30.63 | | |
| | I, B | В | 0.9663 | 37.21 | | | 0.9602 | 34.94 | | |
| | I, F | F | 0.9502 | 35.63 | | | 0.9376 | 32.38 | | |
| | I, H | Н | 0.8886 | 29.88 | | | 0.9171 | 32.01 | | |
| | вент | В | 0.9662 | 37.37 | 0.0204 | 33.02 | 0.9482 | 35.34 | | 32.64 |
| FL-MR | | F | 0.9404 | 35.25 | | | 0.9306 | 32.19 | 0.0238 | |
| I L-MIX | D, 1, 11, 1 | Н | 0.8732 | 30.03 | 0.7274 | 55.72 | 0.9021 | 31.74 | 0.7250 | |
| | | Ι | 0.9379 | 33.03 | | | 0.9145 | 31.29 | | |
| | | В | 0.9676 | 37.57 | | | 0.9630 | 35.85 | | 22.12 |
| FI MPCM | вент | F | 0.9475 | 35.57 | 0 0381 | 3/1/ | 0.9385 | 32.69 | 0.0373 | |
| FL-WIKCM | D , Г , П , I | Η | 0.8940 | 30.27 | 0.9361 | 34.14 | 0.9232 | 32.44 | 0.9373 | 55.15 |
| | | Ι | 0.9432 | 33.13 | | | 0.9244 | 31.54 | | |
| | | В | 0.9698 | 37.62 | 0.9440 | 34.35 | 0.9655 | 35.83 | 0.9398 | 33.14 |
| Mix | | F | 0.9558 | 36.15 | | | 0.9435 | 32.82 | | |
| (Upper | В, F, H, I | Н | 0.9047 | 30.57 | | | 0.9236 | 32.47 | | |
| Bound) | | Ι | 0.9454 | 33.08 | | | 0.9266 | 31.44 | | |