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Human Motion Prediction under Unexpected Perturbation

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Abstract

We investigate a new task in human motion prediction, which is predicting motions under unexpected physical perturbation potentially involving multiple people. Compared with existing research, this task involves predicting less controlled, unpremeditated and pure reactive motions in response to external impact and how such motions can propagate through people. It brings new challenges such as data scarcity and predicting complex interactions. To this end, we propose a new method capitalizing differentiable physics and deep neural networks, leading to an explicit Latent Differentiable Physics (LDP) model. Through experiments, we demonstrate that LDP has high data efficiency, outstanding prediction accuracy, strong generalizability and good explainability. Since there is no similar research, a comprehensive comparison with 11 adapted baselines from several relevant domains is conducted, showing LDP outperforming existing research both quantitatively and qualitatively, improving prediction accuracy by as much as 70%, and demonstrating significantly stronger generalization.

1. Introduction

Human motion prediction aims to predict the future movements given the past motions, which has been heavily studied in computer vision [17, 67–69]. Deviating from existing research, we are interested in a new task setting: predicting human motions, on both individual and group levels, under unexpected physical perturbation. On the individual level, physical perturbation causes reactive motions as opposed to active motions. On the group level, such perturbations can propagate through people while possibly being intensified, *e.g.* a push at the back of a line of people could be transferred all the way to the front. These motions have not been investigated. Incorporating physical perturbation potentially extends motion prediction to new application domains *e.g.* balance recovery in biomechanics [4, 18], reactive motions for character animation [3, 14], crowd crush induced by pushing [6, 53], humanoid robots [24, 26], *etc*.

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Incorporating physical perturbation in prediction imposes new challenges. First, the motions are purely reactive and less controlled such that they are less smooth and less coordinated among body parts. Furthermore, this perturbation can propagate through people when they are packed and the space to recover balance is restricted, such that an attempt to recover balance relies on pushing others. Last but not least, unlike existing research, the data for motion prediction under perturbation is extremely scarce. Not only is it rare to capture full-body motions under such circumstances, but it is also difficult to record the interactions between people, *e.g.* forces of pushes.

Before deep learning, many areas have formulated this problem, which can be broadly divided into two categories. The first is physics-based where human bodies are simplified into connected rigid bodies [37, 53]. The reaction to push is solved via optimization to compute what forces are needed to recover balance [40, 42], or through carefully tuning feed-forward controllers [37, 38]. These methods, despite aiming to mimic the balance recovery of humans, do not learn from human data and therefore cannot predict human motions. Alternatively, reactions to perturbation can be learned from data via regression [60], optimization [66], or reinforcement learning [63]. Comparatively, this type of method tends to generate more human-like motions, but they are not designed for prediction.

Recently, deep learning [44, 56, 67, 68] have dominated human motion prediction, but they cannot be adapted for our problem. First, most datasets only contain single-body motions without external perturbation. Even when multiple people are captured, it is not under unexpected perturbation. To predict push propagation, one would still need to measure information *e.g.* contact forces between people, ground friction, muscle forces, *etc.*, which are all absent. This data scarcity essentially rules out most deeplearning methods. Furthermore, there is also little work in modelling the physical/bio-mechanical interactions that can potentially propagate through people. Current research includes motion forecasting, generation and synthesis. Most

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motion forecasting methods [17, 33, 67] are for a single person, with a few recent exceptions [44, 68, 69] but not involving perturbation. Alternatively, our problem could be formulated as motion generation conditioned on external perturbation. However, current methods [8, 46, 49–51, 73] again do not explicitly model close interactions among multiple people caused by perturbation. Theoretically, motion synthesis [36, 54, 55, 64] is a possibility, which potentially can predict motions under perturbation. But they require dense control signals to guide the synthesis, or/and extensive physical simulation. Therefore, it requires manual labor or/and is difficult to scale to many people.

To address the aforementioned challenges, we need a model that has high data efficiency, strong generalizability and can model interactions between people. In other words, this model needs to be able to learn from a small number of samples, can predict accurately in situations similar to the data, and is capable of generating plausible motions in drastically different scenarios. To this end, we propose a new deep-learning model for human motion prediction under unexpected perturbation. To address the data scarcity, we propose a scalable differentiable physics (DP) model for the human body, to learn the balance strategy and interaction propagation between people, inspired by recent DP research [15, 59, 71]. However, naively following existing DP approaches means we would need to make the full-body simulation differentiable for each individual. Not only is motion intrinsically indifferentiable due to e.g. foot contact, but full-body physical models are too computationally expensive to scale. Therefore, we propose a latent DP space where the full-body physics is reduced into a differentiable inverted pendulum model (IPM) [19, 25, 29, 41], and the full-body poses are mapped to and recovered from the IPM. At the low level, the IPM governs body physics and learns key forces such as ground friction and balance recovery. As the IPM is simple, the required data is small. At the high level, we use neural networks to recover the full-body pose from the IPM, which also does not require much data as the IPM provides strong guidance. We refer to our model as the Latent Differentiable Physics (LDP) model. Note different from other latent physics models where the dimensionality reduction is implicit [47, 62], ours is explicit and physically meaningful (*i.e.* mapping from full-body to IPM).

We show LDP can learn from very limited data and perform well under many widely used metrics. Since there is no similar work to our best knowledge, we adapt a wide range of baseline methods in the most relevant areas (motion forecasting, motion generation and motion synthesis), in single-person and multi-people scenarios, for comparison. The results demonstrate that LDP outperforms them both quantitatively and qualitatively. Notably, our model exhibits remarkable generalizability. It can accommodate unseen out-of-distribution perturbations, group sizes, and group formations, potentially extending our research beyond human motion prediction into broader areas, *e.g.* crowd simulation. Furthermore, owing to the explicit physics model, our model possesses a distinctive feature: explainability, providing plausible explanations for the predicted motion. Formally, our contributions include:

- A new task: human motion prediction under unexpected perturbation. To our best knowledge, this is the first deep-learning paper addressing this problem.
- A novel differentiable physics model in human motion prediction that explicitly considers physical interactions.
- A new differentiable IPM model that learns body physics under complex interactions.
- A novel differentiable interaction model that can learn interactions and interaction propagation.

2. Related Work

Human Motion Prediction. Compared with traditional statistical machine learning [31, 57], deep learning has dominated human motion prediction recently. It can be formulated as a sequence-to-sequence task modelled by Recurrent Neural Networks [13, 22, 43]. Also, human skeletons can be seen as graphs so that spatio-temporal graph convolutions can be employed [9, 10, 33, 34, 72]. Transformer-based methods [1, 5] use the attention mechanism to capture spatial and temporal correlations. Recently, there has been a surge of interest in multi-people motion prediction [44, 58, 68, 69]. MRT [58] models the social interactions between humans via a global encoder. JRFormer [68] exploits the joint relation representation for modelling the interactions where physical interactions are considered implicitly. However, existing methods share a common limitation - they do not consider unexpected perturbations, restricting their applications in predicting actively planned/controlled motions. Additionally, explicit physical interactions between people have often been overlooked in these methods. Our model extends the research to a more challenging scenario involving unexpected perturbation and perturbation propagation. The explicit physics knowledge in our model enables it to achieve better prediction, generalizability, and explainability.

Traditional Research on Balance Recovery Relevant research has been conducted in other fields where traditional methods mainly focus on modelling balance recovery strategies in response to perturbations [4, 6, 18, 24, 26, 42]. Brodie *et al.* [4] analyzed the biomechanical mechanisms in the balance recovery following an unexpected perturbation such as trips and slips. Chen *et al.* [6] studied the dynamics of individuals under pushing in crowds. A new controller was proposed to recover balance for bipedal robots under perturbation [42]. In parallel, some traditional methods aim to synthesize reactive motions to perturbation [3, 39, 40, 45, 60]. Arikan *et al.* [3] proposed an al-



Figure 1. Overview of our model. Given a frame X_t , it is first mapped into the IPM space via Skeleton-to-IPM to get its IPM state I_t . Then I_t is simulated for one step via Differentiable IPM to compute I_{t+1} . Lastly, the full-body frame X_{t+1} is recovered from I_{t+1} via Skeleton Restoration Model. The IPM is shown in the right figure. The full-body state X is represented by joint positions.

gorithm for selecting and adjusting the motions from data to synthesize the motion for animating virtual characters being pushed. [39, 45] explored how to turn the given motions under perturbation into physically valid ones. Overall, traditional methods cannot predict motions under perturbation, either because they do not learn from data or have limited learning capacity. By contrast, we incorporate DP with deep neural networks to predict such human motions.

Differentiable Physics. DP is an emerging field focusing on combining traditional physics models with deep learning techniques, to provide high data efficiency and explainability. Consequently, many domains have investigated differentiable physics such as robotics [7, 30, 61], physics [20, 23], computer vision [70, 71], and computer graphics [15, 35]. We propose the first explicit latent differentiable physics model for human motion prediction under unexpected physical perturbation.

3. Methodology

Problem Definition. Given a motion with multiple people, we denote the skeletal pose of the *n*th person at frame *t* as $X_t^n \in \mathbb{R}^{J \times 3}$ where *J* is the joint number. Unlike existing research aiming to predict *p* frames $\{\hat{X}_{T-p+1:T}^n\}_{n=1}^N$ given *k* frames $\{X_{1:k}^n\}_{n=1}^N$ history, we minimize the required history due to limited data. Given the initial frame $\{X_0^n\}_{n=1}^N$ and the input forces F^{input} , we aim to predict the following T frames, by solving an initial problem:

$$\{\hat{X}_{1:T}^n\}_{n=1}^N = \mathcal{S}_{\gamma}(\{X_0^n\}_{n=1}^N, IPM_{\eta}(\mathcal{M}(\{X_0^n\}_{n=1}^N), F^{input})) \quad (1)$$

where $\{\hat{X}_{1:T}^n\}_{n=1}^N$ is the predicted T frames. \mathcal{M} is a Skeleton-to-IPM mapping $\mathcal{M}: \mathcal{X} \to \mathcal{I}$ where \mathcal{X} and \mathcal{I} are the state space of skeleton poses (represented by joint positions) and the IPM respectively. IPM_{η} is a Differentiable IPM with learnable parameters η . Finally, S_{γ} is the inverse mapping, *i.e.* Skeleton Restoration Model, $S_{\gamma}: \mathcal{I} \to \mathcal{X}$, reconstructing full-body skeleton pose from IPM states, with learnable parameters γ . An overview of our model is shown in Fig. 1. Given a motion, we map the full-body poses

into their corresponding states of an IPM [19, 25, 29] as $\{I_0^n\}_{n=1}^N = \mathcal{M}(\{X_0^n\}_{n=1}^N)$. By simulating the IPM forward in time via IPM_η , it can learn the key parameters η . The interaction forces between people are also learned simultaneously. Meanwhile, our Skeleton Restoration Model S_γ recovers the full-body poses from the predicted IPM states from IPM_η . For training, we minimize the mean squared error (MSE) between the predicted $\{\hat{X}_{1:T}^n\}_{n=1}^N$ and the ground-truth poses $\{X_{1:T}^n\}_{n=1}^N$:

$$Loss = MSE(\{\hat{X}_{1:T}^n\}_{n=1}^N, \{X_{1:T}^n\}_{n=1}^N)$$
(2)

where we need to specify S_{γ} , IPM_{η} and \mathcal{M} in Eq. (1). We give key equations and model information below and refer the readers to the supplementary material (SM) for details.

3.1. Latent Physics Space for Full-body Motions

3.1.1 Background and Skeleton-to-IPM Mapping

We first introduce IPM_{η} and \mathcal{M} in Eq. (1). Differentiable physics (DP) has shown extremely high data efficiency because physics can act as a strong inductive bias and eliminates the reliance on large amounts of training data [11, 59, 71]. For our model, a key design choice is to choose a DP model that has the right level of granularity while being scalable. Among many possible choices from full-body physics [2] to simple rods [65], we choose the Inverted Pendulum Model (IPM) [19, 25, 29] as it can fully capture balance loss and recovery while being scalable.

Our IPM has a massless rod mounted to a cart with a point mass at the end of the rod (Fig. 1 right). Denoting its state $\mathcal{I} \ni I_t = [x_t, y_t, \theta_t, \phi_t] \in \mathbb{R}^4$ at time step t where [x, y] is the coordinates of the cart in the xy-plane and $[\theta, \phi]$ is the rotation angles of the rod around Y_L axis and X_L axis in the local coordinate system Σ_L , respectively. Our full-body pose X is represented by 22 joint positions. \mathcal{M} in Eq. (1) is defined as (Fig. 1 left): the hip joint is mapped onto the point mass, and the midpoint between the two ankle joints is mapped onto the center of the cart. The point mass and the cart jointly determine the two angles $[\theta, \phi]$. Next, IPM_{η} is defined. Given the initial IPM state, we can simulate it in time by solving Eq. (3) repeatedly [41]:

$$M(I_t, l_t)\ddot{I}_t + C(I_t, \dot{I}_t, l_t) + G(I_t, l_t) = F_t^{net}$$
(3)

where $M \in \mathbb{R}^{4 \times 4}$, $C \in \mathbb{R}^{4 \times 1}$ and $G \in \mathbb{R}^{4 \times 1}$ are the inertia matrix, the Centrifugal/Coriolis matrix, and the external force such as gravity, which are all functions of state I_t , its first-order derivative \dot{I}_t and the rod length l_t . While the standard IPM has a fixed rod length, we allow it to change as the distance between the hip and the middle of two ankles can drastically change in human motions. Therefore, we also predict l_t at each time step. Overall given the net force $F_t^{net} \in \mathbb{R}^4$ and the rod length l_t , we can solve Eq. (3) for the next state I_{t+1} via a semi-implicit scheme $\dot{I}_{t+1} = \dot{I}_t + \Delta t \ddot{I}_t$ and $I_{t+1} = I_t + \Delta t \dot{I}_{t+1}$, where Δt is the time step.

Finally, the learnable parameters η in IPM_{η} parameterize F_t^{net} and the rod length l_t , where the formulation differs between single-person and multi-people, and will be elaborated later. It's notable that F_t^{net} in Eq. (3) is the generalized force. Using the generalized force (instead of the Euler force) keeps the motion equation simple, and its entries have explicit physical meanings as shown later.

3.1.2 Single-Person Prediction via Differentiable IPM

Under single-person, we only consider Balance-Recovery and Friction (blue blocks in Fig. 1 Differentiable IPM) when predicting F^{net} . Specifically, we consider three forces:

$$F_t^{net} = F_t^{self} + f_t + F_t^{input} \tag{4}$$

where F_t^{self} , f_t , and F_t^{input} are the balance recovery force, the ground friction and the external perturbation. The Balance-Recovery module learns F_t^{self} which is further decomposed into $F_t^{self} = F_t^{self-pd} + F_t^{self-nn}$. This decomposition is because F_t^{self} is the muscle force at the hinge of the rod which serves two purposes. The first one is to give a feed-forward torque $F_t^{self-pd}$ to react to perturbation for balance recovery, and the second is to give a torque correction $F_t^{self-nn}$ for tracking observed motions. In generalized forces, we parameterize $F_t^{self-pd}$ by proportional derivative (PD) control:

$$F_t^{self-pd} = K_p e_t + K_d \dot{e}_t, e_t = s_d - s_t$$
(5)

where e_t is the PD state error, K_p and K_d are the control parameters. Different from the IPM state, the current PD state is $s_t = [\dot{x}_t, \dot{y}_t, \theta_t, \phi_t]$ and the desired PD state s_d is [0, 0, 0, 0]. In other words, we assume people tend to recover to the upright body pose and zero linear velocity after unexpected perturbation, which is a widely accepted assumption [28, 32, 48]. However, $F_t^{self-pd}$ only captures the general balance recovery strategy. To mimic the data, we parameterize $F_t^{self-nn}$ with a Long Short Term Memory (LSTM) network:

$$F_t^{self-nn} = LSTM([\theta_t, \phi_t, \dot{x}_t, \dot{y}_t, \dot{\theta}_t, \dot{\phi}_t, M]), \quad (6)$$

where M is the mass of the person.

Ground friction f_t is the main reason for successful selfbalance and therefore needs to be explicitly considered. In generalized forces, friction affects the IPM motion via damping [41]. So we parameterize $f_t = -\mu[\dot{x}_t, \dot{y}_t, 0, 0]$, where the parameter μ is a learnable positive scalar and shared by all people for simplicity. The damping force only directly influences the cart motion. Finally, to compute Eq. (3), we also need to predict the change of the rod length l_t , where we employ a multi-layer perception (MLP):

$$\Delta l_t = MLP([\theta_t, \phi_t, \dot{x}_t, \dot{y}_t, \dot{\theta}_t, \dot{\phi}_t, F_t^{self}, M, l_t])$$
(7)

where l_t is the rod length at time step t. We predict the rod length at the next time step by $l_{t+1} = l_t + \Delta l_t$. Finally, after obtaining the prediction of F_t^{net} and l_t at every time step t, we can calculate the next IPM state by solving Eq. (3) via the semi-implicit scheme mentioned above.

3.1.3 Multi-people with Differentiable Interaction

When there is more than one person, the complexity increases quickly. The main reason is that the interaction propagation among people is: (1) complex, *e.g.* complicated contact positions/duration/forces. (2) hard to capture in data. Therefore, we propose to consider them as latent variables that cannot be directly observed. But again large amounts of data would be needed if we only relied on data to infer these variables. Therefore we model the interactions in the reduced IPM space, rather than the original space, so that it becomes a Differential Interaction Model (DIM).

Our DIM models a differentiable interaction force between any two IPMs and is learned in the Interaction module (the yellow block in Fig. 1 Differentiable IPM). The overall net force on an IPM in multi-people then becomes:

$$F_t^{net} = F_t^{self} + F_{t,n}^{inta} + f_t + F_t^{input}$$
(8)

where F_t^{self} , f_t and F_t^{input} are the same as Eq. (4). Note all forces are learned and shared among all people, so that we can generalize to an arbitrary number of people later. $F_{t,n}^{inta} \in \mathbb{R}^4$ is the new interaction force:

$$F_{t,n}^{inta} = \sum_{j \in \Omega_{t,n}} F_{t,nj}^{inta} = \sum_{j \in \Omega_{t,n}} F_{t,nj}^{inta-bs} + F_{t,nj}^{inta-nn}$$
(9)

where $\Omega_{t,n}$ is the neighborhood of the person n at time t. $F_{t,nj}^{inta}$ is the interaction force applied onto person n from her/his neighbor $j \in \Omega_{t,n}$. We model two factors in $F_{t,nj}^{inta-bs}$ and $F_{t,nj}^{inta-nn}$. The first $F_{t,nj}^{inta-bs}$ represents a consistent and trackable repulsive tendency when

two IPMs get close, while $F_{t,nj}^{inta-nn}$ captures the variations of the repulsion. So we expect $F_{t,nj}^{inta-bs}$ to capture most of the interaction while $F_{t,nj}^{inta-nn}$ being a supplement. To this end, we separate the dimensions of an IPM state $I = [x, y, \theta, \phi]$ into two groups [x, y] and $[\theta, \phi]$ and treat them separately as $F_{nj}^{bs-xy} \in \mathbb{R}^2$ and $F_{nj}^{bs-\theta\phi} \in \mathbb{R}^2$, such that $F_{t,nj}^{inta-bs} = [F_{nj}^{bs-xy}, F_{nj}^{bs-\theta\phi}]^{T}$, where we omit the time subscript t and the superscript *inta* for simplicity.

For F_{nj}^{bs-xy} , we define a repulsive potential energy between two close IPMs which leads to a repulsive force:

$$F_{nj}^{bs-xy}(r_{nj}) = -\nabla_{r_{nj}}\mathcal{U}[b(r_{nj})], \ \mathcal{U}[b] = ue^{-\frac{b}{\sigma}}$$
(10)

$$b = \frac{1}{2}\sqrt{(\|r_{nj}\| + \|r_{nj} - \triangle t\dot{r}_{jn}\|)^2 - \|\triangle t\dot{r}_{jn}\|^2}.$$
 (11)

where $r_{nj} = r_n - r_j$ is the relative position of the carts of a person and his/her neighbor j, *i.e.* r_n is the vector [x, y]in the IPM state I_n . The $\mathcal{U}[b]$ is the repulsive potential with elliptical equipotential lines, and u and σ are hyperparameters. b is the semi-minor axis of the ellipse where $\dot{r}_{jn} = \dot{r}_j - \dot{r}_n$ is the relative velocity. For $F_{nj}^{bs-\theta\phi}$, we treat it as a force with a constant mag-

For $F_{nj}^{bs-\theta\phi}$, we treat it as a force with a constant magnitude (tunable hyperparameter) and apply it on θ and ϕ independently. Although the magnitude is constant, its directions can vary in different situations. We explain it for θ and the same principle applies to ϕ . On the high level, we need to decide the direction of $F_{nj}^{bs-\theta\phi}$ based on the states of two close IPMs. θ can be positive, zero and negative. For two IPMs, this produces a total of 9 possible states, which we detail in the SM.

After defining $F_{t,nj}^{inta-bs}$, we explain $F_{t,nj}^{inta-nn}$ which should capture the variation of interactions. Unlike $F_{t,nj}^{inta-bs}$ where we can define an explicit form, we learn $F_{t,nj}^{inta-nn}$ via an MLP:

$$F_{nj}^{nn} = MLP([x_{nj}, y_{nj}, \theta_n, \phi_n, \theta_j, \phi_j, \dot{x}_{nj}, \dot{y}_{nj}, \dot{\theta}_{nj}, \dot{\phi}_{nj}]) \quad (12)$$

where $x_{nj} = x_n - x_j$ and $\dot{x}_{nj} = \dot{x}_n - \dot{x}_j$. y_{nj} , \dot{y}_{nj} , θ_{nj} and $\dot{\phi}_{nj}$ are computed in a similar fashion.

3.2. Skeleton Restoration Model

To predict full-body motion, we recover the full-body pose from the predicted IPM states. This is divided into two steps as shown in Fig. 1. We first recover the lower body from the IPM state, then recover the upper body from both the IPM state and the recovered low body. There are two reasons for this design. First, the Skeleton-to-IPM mapping dictates that the IPM has a higher correlation with the lower body than with the upper body. Also, the dynamics of the lower body and the upper body are relatively independent [27, 49], *i.e.* similar low-body motions can correspond to different upper-body motions, *e.g.* different styles in walking. Therefore, we use two models to recover the lower body and the



Figure 2. FZJ Push [12]. The blue agent was pushed by the punch bag and then he pushed other people.

upper body, respectively. Overall, although the Skeleton Restoration Model involves deep neural networks, the required data is small as there is strong IPM guidance.

Lower Body Restoration. We use a Conditional Variational Autoencoder (CVAE) [46, 49, 64] (CVAE-Lower in Fig. 1) to learn a Normal distribution of the lower body X_{t+1}^l in the latent space conditioned on X_t^l . During inference, since X_{t+1}^l is unavailable, we train a sampler (Lower Sampler) to sample the latent space to generate the next frame \hat{X}_{t+1}^l . The Lower Sampler network is an MLP. It takes as input X_t^l , I_{t+1} , and outputs a latent code of CVAE-Lower takes as input the current lower body X_t^l and the predicted IPM state I_{t+1} , to predict the next lower body \hat{X}_{t+1}^l , essentially reconstructing the lower body under the IPM guidance.

Upper Body Restoration. Similarly, we also use a CVAE named CVAE-Upper, except this time we use both the lower body predicted by CVAE-Lower \hat{X}_{t+1}^l and the current upper body X_t^u as the condition. A sampler (Upper Sampler) is also used to take as input I_{t+1} , \hat{X}_{t+1}^l and X_t^u , and sample the latent space of CVAE-Upper, which is then decoded to predict the upper body at the next frame \hat{X}_{t+1}^u .

3.3. Training with Auxiliary Losses

In summary, the learnable parameters of our model include: the LSTM (Eq. (6)), the MLPs (Eq. (7), Eq. (12)), the ground friction coefficent μ , CVAE-Lower, CVAE-Upper, Lower Sampler and Upper Sampler. Other than the main loss in Eq. (2), we also use other auxiliary losses such as foot sliding, IPM state MSE, *etc.* We also pre-train some components for initialization. Due to space limit, all details including training/prediction algorithms, implementation details, parameters, code, data, *etc.* are in the SM.

4. Experiments

4.1. Dataset and Metrics

Data for our problem is extremely scarce compared with other human motion prediction research. The only publicly available dataset, to our best knowledge, is a new dataset



Figure 3. Perturbations with different magnitudes in single-person (top) and multi-people (bottom).

| Method | MPJPE | hipADE | hipFDE | MBLE | FSE |
|-----------|-------|--------|--------|-------|-------|
| A2M | 0.403 | 0.386 | 0.730 | 0.019 | 0.200 |
| ACTOR | 0.362 | 0.338 | 0.591 | 0.020 | 0.434 |
| MDM | 0.500 | 0.424 | 0.686 | 0 | 2.567 |
| RMDiffuse | 0.228 | 0.202 | 0.299 | 0.011 | 0.790 |
| PhyVae | 0.260 | 0.249 | 0.460 | 0.009 | 0.170 |
| siMLPe | 0.130 | 0.117 | 0.226 | 0.006 | 0.182 |
| EqMotion | 0.296 | 0.270 | 0.543 | 0.064 | 1.552 |
| Ours | 0.097 | 0.086 | 0.171 | 0.002 | 0.131 |
| MRT | 0.162 | 0.140 | 0.282 | 0.010 | 0.256 |
| DuMMF | 0.312 | 0.285 | 0.480 | 0 | 3.194 |
| TBIFormer | 0.204 | 0.177 | 0.305 | 0.010 | 0.234 |
| JRFormer | 0.181 | 0.152 | 0.260 | 0.012 | 0.932 |
| Ours | 0.106 | 0.092 | 0.218 | 0.003 | 0.069 |

Table 1. Metrics in single-person (top) and multi-people (bottom).

[12] named FZJ Push. The dataset includes standing individuals, groups of four, and groups of five, with one person pushed by a punching bag unexpectedly and the push is propagated through the group. In total, the dataset includes only 45 single-person motions and 63 multi-people motions. This is considerably less than data normally used for human motion prediction. As shown later, the necessity of a model with high data efficiency is crucial. The motion is recorded at 60 Hz. Shown in Fig. 2 a, a hanging punch bag is operated by a person to give pushes of various magnitudes to one person in the group. Then the skeletal motions (Fig. 2 b) are recorded. There is a pressure sensor measuring the pushing forces on the punching bag. However, the pushing forces between people are not recorded. We discard redundant data such as frames in waiting.

For evaluation, we adopt five widely used metrics [49, 67, 69]: Mean Per Joint Position Error (MPJPE) in meters, Average Displacement Error at the hip (hipADE) in meters, Final Displacement Error at the hip (hipFDE) in meters, Mean Bone Length Error (MBLE) in meters, and Foot Skating Error (FSE) in centimeters. Details and justifications for these metrics are in the SM.

4.2. Baselines

There is no similar work in human motion prediction to our best knowledge, so we carefully review a wide spectrum of research in motion prediction, synthesis and generation, and choose the latest methods in each field for comparison. Specifically, we choose 11 baselines: A2M [16], ACTOR [46], MDM [51], RMDiffuse [73], PhyVae [64], siMLPe [17] and EqMotion [67] for the single-person scenario, and MRT [58], DuMMF [69], TBIFormer [44] and JRFormer [68] for the multi-people scenario. The specific adaptation varies according to the baseline, and we give the details in the SM. One notable difference is our model only requires the first frame with the perturbation force during inference, while the other methods tend to require much more information such as multiple frames.

4.3. Quantitative Results

The single-person comparison is shown in Tab. 1 top. Despite requiring the minimal information, our model still achieves the best performance on all metrics except the MBLE. MDM obtained 0 MBLE because its parameterization is joint angle based, *i.e.* no bone-length change incurred. A joint angle parameterization could also work with our model but in practice, we find a joint-positionbased parameterization works better. Across different metrics, LDP outperforms the best baseline by as much as 25.38%, 26.50%, 24.34%, 66.67%, and 22.94% on MPJPE, hipADE, hipFDE, MBLE, and FSE respectively, excluding the MBLE of MDM. We tend to attribute the higher performance to the explicit physics-based inductive biases embedded in the design of LDP. Furthermore, we look into performances under perturbations with different magnitudes (weak, medium and strong) in Fig. 3 top, where we only include the best three baselines and leave the full comparison in SM. Stronger pushes lead to stronger responses and tend to be harder to predict. This is especially obvious in metrics related to motion tracking, i.e. MPJPE, hipADE and hipFDE, where as the push becomes stronger, the errors become larger. Comparatively, LDP consistently outperforms other baselines, demonstrating its effectiveness in strong perturbations. In addition, compared with weak and medium pushes, LDP has a slower error increment under



Figure 4. Visual Results in the Single-person scenario.

strong pushes, in contrast to the more volatile performances of other baselines, showing better generalizability. Overall, LDP either ranks as the best or is close to the top performance across metrics and perturbation levels.

The results under the multi-people scenario are shown in Tab. 1 bottom. The MBLE of DuMMF is 0 because it employs joint-angle-based parameterization. Multi-people is a challenging task for all methods. On all metrics, LDP outperforms all baselines by at least 34.57%, 34.29%, 16.15%, 70%, and 70.51% on MPJPE, hipADE, hipFDE, MBLE, and FSE, respectively, (excluding the MBLE of DuMMF). Moreover, we show detailed analysis under perturbations with different magnitudes in Fig. 3 bottom, with the three best baselines. One challenge in multi-people is to predict the onset and duration of interactions. The baseline methods need to learn the interactions by purely fitting the data, while our method learns them as a latent physical process. Consequently, none of the baselines can predict well, *e.g.* they predict moving without being pushed or not moving while being pushed, while our model can learn to predict the interactions and their propagation well. Overall, our model achieves or is close to the best performance across metrics and perturbation levels.

4.4. Qualitative Results

We visually compare our methods with the best three baselines under single-person in Fig. 4. Our prediction has the highest quality and is the most similar to the ground truth. RMDiffuse severely violates bone lengths, especially around ankles, and generates jittering motions. PhyVae predicts walking but with rather small steps. siMLPe predicts only a single step. The multi-people scenario is much harder (Fig. 5), where both individual reactions and interactions need to be predicted. MRT and TBIFormer suffer

| Method | MPJPE | hipADE | hipFDE | MBLE | FSE |
|----------------|-------|--------|--------|-------|-------|
| no IPM, Full | 0.217 | 0.195 | 0.341 | 0.007 | 0.196 |
| no IPM, Low-up | 0.206 | 0.184 | 0.320 | 0.009 | 0.313 |
| IPM, Full | 0.110 | 0.094 | 0.242 | 0.004 | 0.126 |
| IPM, Low-up | 0.106 | 0.092 | 0.218 | 0.003 | 0.069 |

Table 2. Ablation study with (1) IPM and no IPM, (2) Full body and Lower-up body pose reconstruction.

from serious intersections between individuals. JRFormer predicts merely subtle movements that deviate considerably from the ground truth. Our model generates the most similar prediction to the ground truth.

Explainability In Fig. 5 bottom, we show the learned net forces on the second person (from left), to provide plausible explanations of the predicted motion. This person remains still initially under zero net force, then experiences a push from the first person, resulting in forces in x and θ , and small forces in y and ϕ . Then the third person is pushed by the second, resulting in the change of the net force on the second person from positive to negative in x and θ . Finally, the second person recovers the balance. Our model predicts the motion results from plausible forces, and therefore possess strong explainability.

4.5. Generalization

LDP can easily generalize to out-of-distribution scenarios, *e.g.* unseen pushes, more people, different formations, *etc.* Since there is no ground truth, we show the visual result of a challenging generalization scenario in Fig. 6, where 13 people stand in a diamond formation and 3 of them indicated by the orange arrows are pushed. Note the data only contain up to 5 people in simple formations such as one or two lines. So this 13-people formation is totally out-of-distribution. However, our model can still generate plausible motions for the entire group, given only the initial poses and the perturbation forces, demonstrating strong generalizability. More experiments can be found in the SM.

4.6. Ablation Study

The Differentiable IPM and the Skeleton Restoration Model are two key components of our model. We conduct the ablation study to assess the effectiveness of them. There are four combinations: with/without IPM, and full-body restoration or separate restoration (first lower body then upper body). When the IPM is absent, the next frame is directly predicted by either one full-body CVAE (Full) or two CVAEs with one for the lower body and the other for the upper body (Low-up). Without IPM, there are also no samplers (Lower Sampler and Upper Sampler in Fig. 1) so we need to directly sample in the latent space of the CVAEs. We randomly sample the latent space 3 times when predicting the next frame



Figure 5. Multi-people comparison. The last row shows the learned net force on the second (from the left) person. The bar height indicates the magnitude and the sign indicates the direction, where the people move in the positive direction of the x-axis.



Figure 6. A 13-person group in a diamond formation with three people (indicated by orange arrows) being pushed.

and average the results. In contrast, with IPM, we can train the samplers to only sample once to predict the next frame.

Results are shown in Tab. 2. When there is no IPM, the performance deteriorates significantly across all metrics. With the IPM guidance, all metrics are significantly improved. Further, the Low-up separation of the body improves the performance further across all metrics under the IPM guidance, especially on the FSE. However, it exhibits limited effectiveness without the IPM guidance, even resulting in a bad FSE. This is because IPM states have strong correlations with the lower body, without which the Low-up is unable to improve the performance significantly even when the lower body is separately predicted.

5. Conclusion

We proposed a new task, human motion prediction under unexpected perturbation, which extends human motion prediction into new application domains. To this end, we have identified and overcome new challenges *e.g.* data scarcity and interaction modelling, by proposing a new class of deep learning models based on differentiable physics. Our model outperforms existing methods despite requiring far less information and shows strong generalization to unseen scenarios. One limitation is our method requires explicit modelling of the physical process, making the model not as general as black-box deep neural nets that can be plug-and-play on data. However, we argue this is mainly driven by the data scarcity. Also, it brings stronger generalizability and interpretability. In future, we will investigate more general physics models that can potentially accommodate more diversified physical interactions between people. A big difference between other existing datasets [21, 52] and the dataset FZJ Push is the former is active motions while the latter is passive balance recovery. We will also explore LDP on action motions in future.

Acknowledgements

The project received funding from the European Union's Horizon 2020 research and innovation programme under grant agreement No 899739 CrowdDNA.

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